

Novel Liposome-Capture Surface Chemistries to Analyze Drug-Lipid Interaction Using the ProteOn™ XPR36 System

Tech
Note

Moran Edri¹, Ruben Luo², Emilia Rabkin¹, Shai Nimri¹, and Dalia Shezifi¹
¹Bio-Rad Laboratories, Inc., 1 Gutwirth Park, Technion, Haifa 32000, Israel
²Bio-Rad Laboratories, Inc., 2000 Alfred Noble Drive, Hercules, CA, USA

Protein Interactions

Bulletin 6449

Abstract

Surface plasmon resonance (SPR) biosensors analyze biomolecular interactions in a label-free and real-time manner. The ProteOn XPR36 protein interaction array system is an SPR platform for analyzing label-free biomolecular interactions. It features a 6 x 6 interaction array to provide versatility in experimental design, high productivity, and high data quality. The ProteOn liposome capturing kit used within the ProteOn XPR36 system provides a novel hydrophilic surface chemistry that allows for advanced applications such as drug-lipid interaction analysis. This kit can be used to evaluate small molecule drug delivery by measuring properties of drugs and assessing drug carrier systems.

Introduction

The ProteOn XPR36 system is an SPR platform that allows for highly efficient optimization of experimental conditions by featuring an array of 6 x 6 biomolecular interactions. The array allows simultaneous probing of six target immobilization conditions in six ligand channels together with six interaction conditions in six analyte channels, shown in Figure 1. The 6 x 6 configuration also enables novel referencing options for high-quality data and high-throughput sample analysis. These advantages position the ProteOn XPR36 system as an optimal SPR platform in label-free drug discovery applications, providing high-quality data, ideal experimental versatility, and excellent cost-effectiveness. Recently, in addition to the traditional protein-protein interaction applications, the ProteOn XPR36 system has contributed to the rapid progression made in exploring novel applications, such as drug-lipid interaction analysis.

ProteOn Lipid Application Kits

Lipid vesicles such as liposomes have been applied in SPR biosensors for analyzing cell membrane-involved biomolecular interactions. Liposomes can be used to construct a lipid bilayer environment, thus this approach facilitates the characterization of cell membrane-related biological factors, such as the partition of small molecule drugs across cell membranes.

In order to apply liposomes in SPR biosensors, a method must be used to capture liposomes on the surface of sensor chips. The conventional method is based on a lipophilic surface chemistry, such as covalently linking alkyl groups to the chip surface to anchor liposomes through lipophilic interactions. Sensor chips or kits now on the market that use this method include the ProteOn GLC lipid kit (Bio-Rad Laboratories, Inc.) and the Biacore L1 sensor chip (GE Healthcare). The workflow for application of the GLC lipid kit is shown in Figure 2. This method is effective in many liposome-based interaction analysis cases. However, its applications are limited by the drawbacks, which include the risk of liposome structure rapture, incomplete surface regeneration, and nonspecific binding of analytes to the lipophilic surface in the following interaction analysis step.

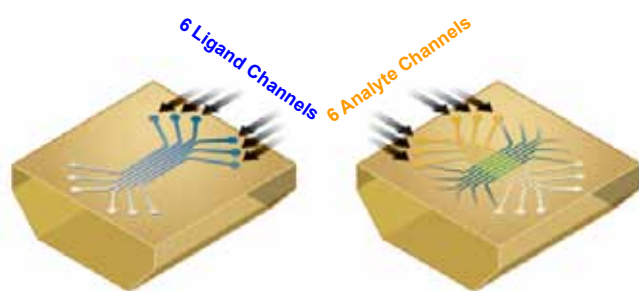


Fig. 1. The ProteOn XPR36 system features an array of 6 x 6 biomolecular interactions realized through forming six ligand channels followed by six perpendicular analyte channels on the surface of a sensor chip. The 6 x 6 configuration enables highly efficient optimization of experimental conditions, novel referencing options for high-data quality, and high-throughput sample analysis.

BIO-RAD

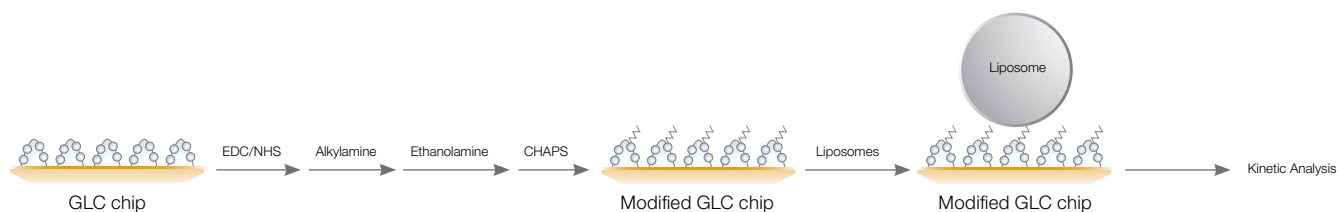


Fig. 2. Workflow for liposome capture using the GLC lipid kit, based on conventional lipophilic surface chemistry.

The ProteOn liposome capturing kit offers a novel method for liposome capture. This kit includes the LCP sensor chip and the LCP capturing reagent kit. The reagent kit offers a uniquely designed cholesterol-tagged, uneven, double-stranded DNA that binds to liposomes through lipophilic interaction. The attachment to the liposomes is very stable, which is attributed to the “bivalent” binding of the two cholesterol moieties. The uneven double-stranded DNA then binds to a single-stranded DNA on the chip surface to anchor the liposomes. Thus, this kit provides a hydrophilic surface chemistry that allows for high-performance liposome capture. The benefits of this method include (1) reduction of nonspecific binding of analytes to the lipophilic chip surface, (2) easy and effective chip surface regeneration by triggering DNA dehybridization, and (3) ability to maintain captured liposomes intact using the double-stranded DNA linker on the chip surface. The workflow for applying the liposome capturing kit is illustrated in Figure 3. Using this kit, it is also possible to form multiple layers of liposomes if high-level liposome capture is desired.

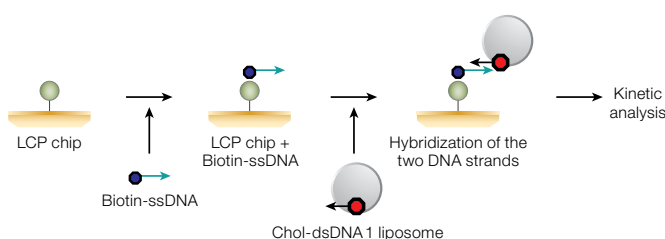


Fig. 3. Workflow for liposome capture using the liposome capturing kit, based on the novel hydrophilic surface chemistry. The LCP chip surface is saturated with single-stranded biotinylated DNA molecules, and liposomes tagged with cholesterol-labeled double-stranded DNA molecules are captured to the surface through DNA hybridization. For reagents and techniques used in this workflow, refer to Bio-Rad bulletin 6161.

Liposome–Small Molecule Drug Interaction Analysis Used as a Drug Delivery Model

Small molecule drugs with ideal efficacy should be both soluble in aqueous solution and able to pass through lipophilic matter such as cell membranes. The balance of hydrophilicity and lipophilicity is an essential aspect in drug delivery because it indicates the drugs intestinal permeability and efficacy to intracellular targets of small molecule drugs.

Thus, in order to optimize that balance during the drug discovery process, many *in vitro* methods to analyze the drug partitioning across cell membranes have been proposed, such as partition coefficient analysis using an equilibrated system of aqueous solution and *n*-octanol (Buchwald and Bodor 1998). However, these methods do not establish an interface of aqueous solution and lipid bilayer structure, thus they may not be able to accurately predict drug transport across biological membranes. Researchers have been analyzing drug partitioning using liposomes, which accurately mimic the lipid bilayer geometry and ionic characteristics of cell membranes, allowing a good correlation to *in vivo* analysis of intestinal permeability of small molecule drugs (Balon et al. 1999). In this report, a variety of liposomes were captured on a sensor chip surface using the ProteOn liposome capturing kit, and small molecule drugs were screened against these liposomes to assess their partitioning characteristics across cell membranes of different types.

Another common application of liposomes is as a drug carrier system to increase the therapeutic index of the delivered drugs. Liposomes filled with ammonium sulfate are an efficient system for active loading of weakly basic small molecule drugs. The formed transmembrane ammonium sulfate gradient creates an acidic pH environment inside the liposomes while the outside bulk solution is at a more neutral pH. When the neutral form (not protonated) of a small molecule drug penetrates into the liposomes, it will become protonated and lose the ability to penetrate the lipid bilayer membranes. Therefore, if the pH inside the liposomes is low enough to protonate basic drugs, and the pH outside the liposomes is likewise higher, the drug will accumulate inside the liposomes (Barenholz 2006).

As a label-free SPR biosensor, the ProteOn XPR36 system is able to directly analyze the interactions between small molecule drugs and liposomes, serving as an ideal platform for the liposome-based *in vitro* characterization of drug partitioning and drug carrier systems (Danelian et al. 2000, Baird et al. 2002).

Screening of the Interactions Between Small Molecule Drugs and Liposomes

Using the 6 x 6 configuration in the ProteOn XPR36 system, five different types of liposomes were captured on the surfaces of the vertical channels (ligand channels) by applying the ProteOn liposome capturing kit as instructed in the product manual (www.bio-rad.com/lcplkit). Fourteen small molecule drugs were injected in the horizontal channels

(analyte channels) in three consecutive steps to screen the interactions between the drugs and the liposomes. The experimental design is shown in Figure 4. The sensorgrams of the interaction analysis are referenced to a blank surface (either a blank ligand channel or interspots) and a blank injection (simultaneous buffer injection in an analyte channel) (Bio-Rad Bulletin 5390). The screening results are shown in Figure 5.

Step 1. Capture of liposomes to chip surface.

PBS

Plain DSPC/CHOL/mPEG2000-DSPE (50:45:5 mol/mol)

DSPC/CHOL (55:45 mol/mol) with 350 mM $(\text{NH}_4)_2\text{SO}_4$

Plain DSPC/CHOL (55:45 mol/mol)

Plain DSPC/CHOL (67:33 mol/mol)

Plain POPC

Step 2. Injection of small molecule drugs (0.5 mM).

Running buffer → Metoprolol → Naproxen

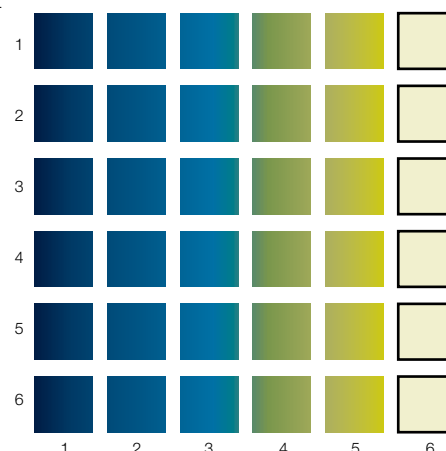
Desipramine → Hydrochlorothiazide → Ketoprofen

Verapamil → Tetracaine → Pindolol

Running buffer → Alprenolol → Tolmetin

Imipramine → Dibucaine → Sulpiride

Propranolol → Running buffer → Running buffer



POPC		DSPC/CHOL (67:33)		DSPC/CHOL (55:45)		DSPC/CHOL (55:45) ($\text{NH}_4)_2\text{SO}_4$		DSPC/CHOL/PEG (50:45:5)	
RU	CV	RU	CV	RU	CV	RU	CV	RU	CV
7,810	0.7%	11,600	0.7%	10,150	0.1%	8,880	0.3%	6,720	0.4%

Fig. 4. The experimental design of the screening of fourteen small molecule drugs against five liposomes using the 6 x 6 configuration in the ProteOn XPR36 system. Five liposomes: plain POPC, plain DSPC/CHOL 67:33 mol/mol, plain DSPC/CHOL 55:45 mol/mol, DSPC/CHOL 55:45 mol/mol with 350 mM $(\text{NH}_4)_2\text{SO}_4$ (DSPC/CHOL $(\text{NH}_4)_2\text{SO}_4$ in abbreviation), and plain DSPC/CHOL/mPEG2000-DSPE 50:45:5 mol/mol. Running buffer: 50 mM NaH_2PO_4 at pH 5.5, 150 mM NaCl, 0.1% DMSO. Abbreviations: PBS — phosphate-buffered saline; POPC — 1-palmitoyl-2-oleoyl-sn-glycero-3-phosphocholine; DSPC — 1,2-distearoyl-sn-glycero-3-phosphocholine; CHOL — cholesterol; mPEG2000-DSPE — 1,2-distearoyl-sn-glycero-3-phosphoethanolamine-N-[methoxy(polyethylene glycol)-2000]. Flow rate was 30 $\mu\text{l}/\text{min}$ for liposome capture and 100 $\mu\text{l}/\text{min}$ for analyte injection. The capture levels of the five liposomes and the column volume (CV) among six interaction spots in each ligand channel are shown in the table. RU, response units.

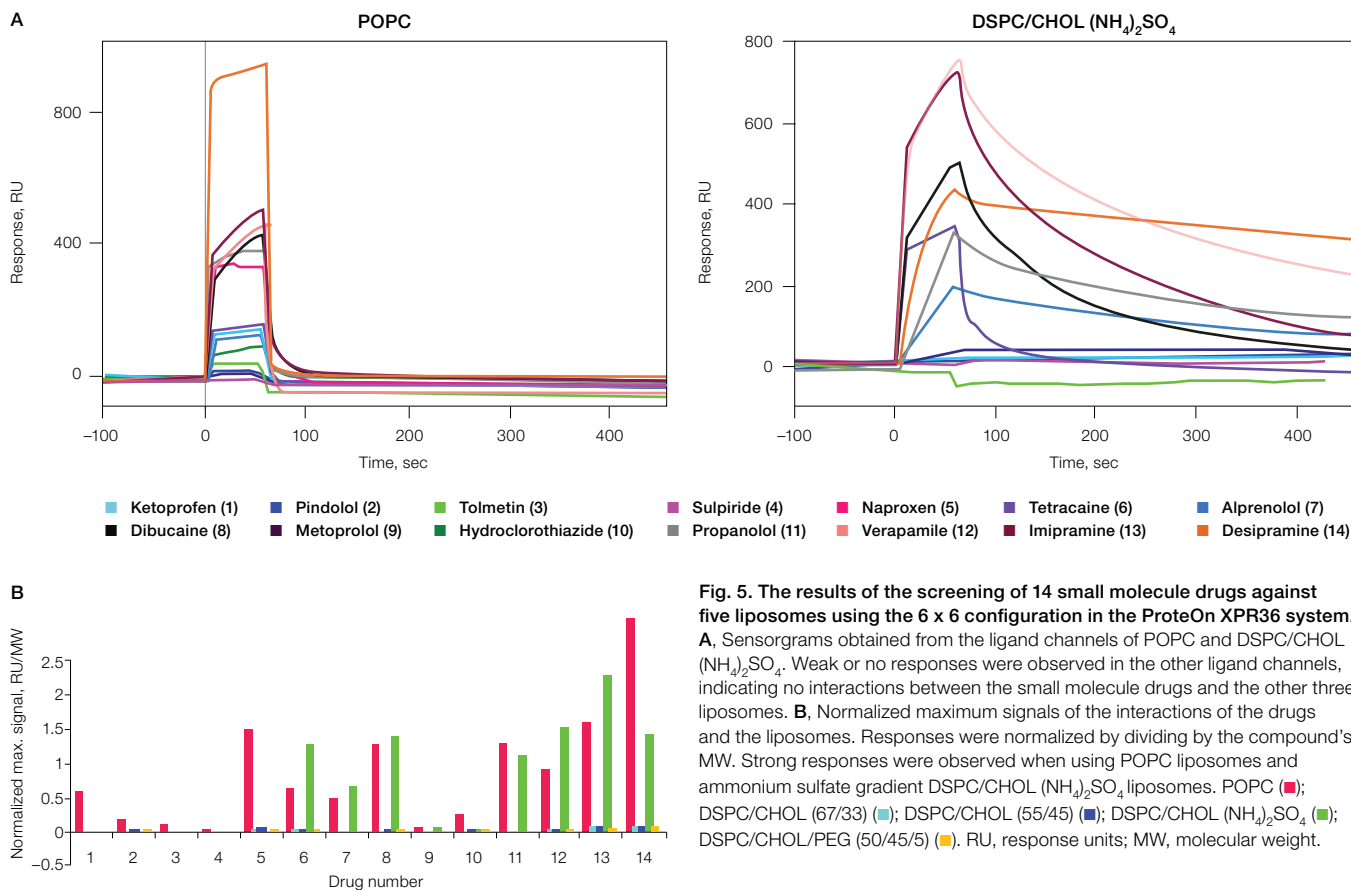


Fig. 5. The results of the screening of 14 small molecule drugs against five liposomes using the 6 x 6 configuration in the ProteOn XPR36 system.

A. Sensorgrams obtained from the ligand channels of POPC and DSPC/CHOL (NH₄)₂SO₄. Weak or no responses were observed in the other ligand channels, indicating no interactions between the small molecule drugs and the other three liposomes. **B.** Normalized maximum signals of the interactions of the drugs and the liposomes. Responses were normalized by dividing by the compound's MW. Strong responses were observed when using POPC liposomes and ammonium sulfate gradient DSPC/CHOL (NH₄)₂SO₄ liposomes. POPC (■); DSPC/CHOL (67/33) (□); DSPC/CHOL (55/45) (■); DSPC/CHOL (NH₄)₂SO₄ (■); DSPC/CHOL/PEG (50/45/5) (■). RU, response units; MW, molecular weight.

The seven compounds that bound to DSPC/CHOL (NH₄)₂SO₄ are weak bases (Drug numbers 6, 7, 8, 11, 12, 13, and 14). The three weak acids did not show binding to this ammonium liposome (Drug numbers 1, 3, and 5). This result is consistent with the theory that weakly basic small molecule drugs are retained in the acidic environment inside the ammonium sulfate gradient liposomes. Four drugs that showed strong interactions with POPC and DSPC/CHOL (NH₄)₂SO₄ were chosen for further dose-response analysis: tetracaine, imipramine, dibucaine, and desipramine.

The four small molecule drugs were prepared in a twofold dilution series ranging from 500 to 31 μM and injected in the analyte channels. The interactions on the 6 x 6 array were measured and the sensorgrams obtained from the ligand channels of POPC and DSPC/CHOL (NH₄)₂SO₄ are shown in Figure 6. The maximum responses in the sensorgrams are plotted against the analyte concentrations and the following facts are observed:

- In most cases, biphasic binding was observed, indicating complex binding mechanisms that may have occurred close to the penetration of drugs into the liposomes. The term biphasic binding means that the observed interaction is composed of fast and slow binding mechanisms.
- Different interaction patterns were observed between the two liposomes: POPC showed fast association and fast dissociation, while DSPC/CHOL (NH₄)₂SO₄ showed biphasic binding and much slower dissociation. In some cases, only the slow phase is observed. This is in agreement with the active loading mechanism — accumulation of drug molecules inside the liposomes when the ammonium gradient is formed.

The results demonstrate that this drug delivery model can be used for the evaluation of drug partitioning across cell membranes.

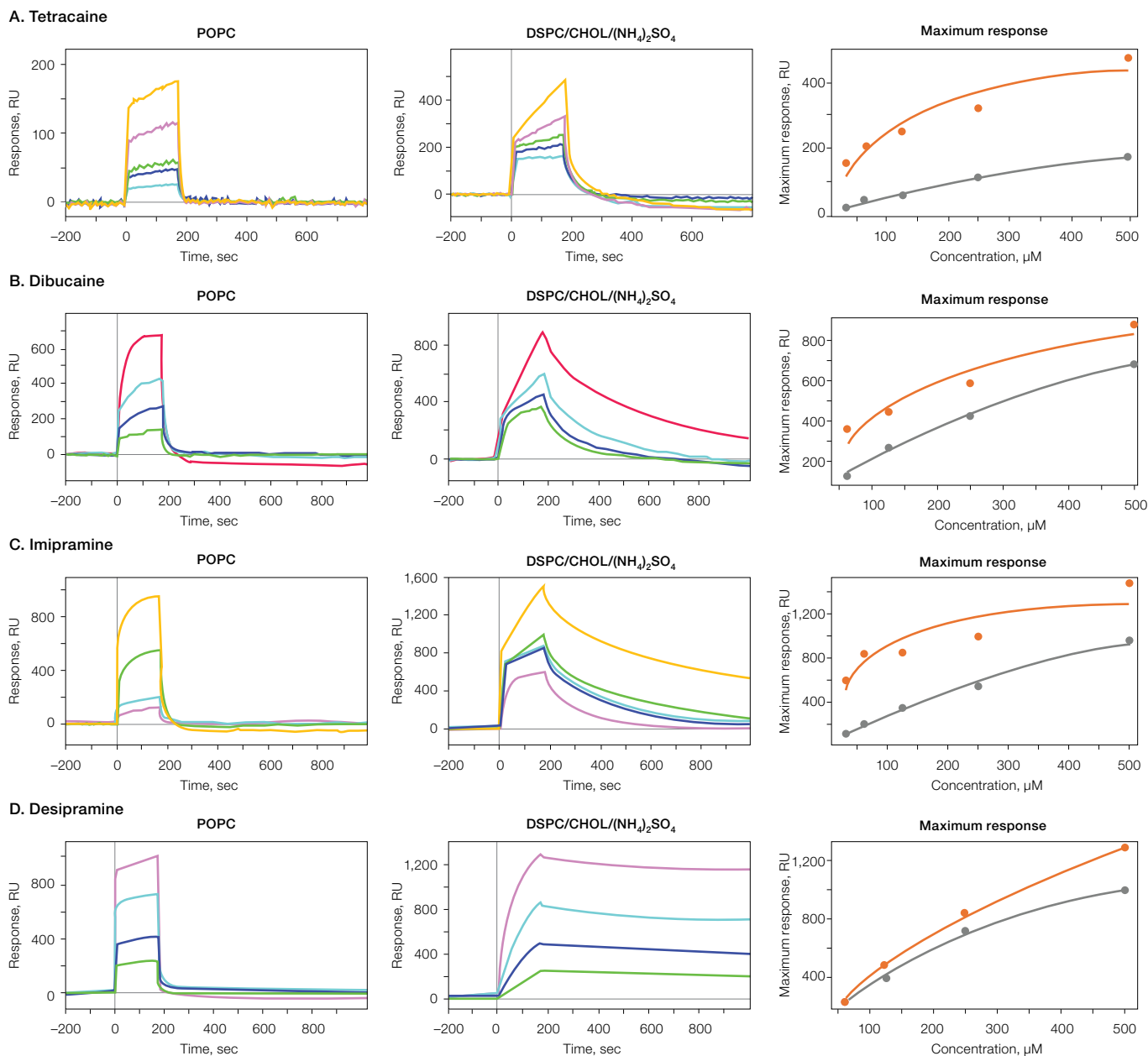


Fig. 6. Dose-response analysis of four small molecule drugs: **A**, tetracaine; **B**, dibucaine; **C**, imipramine; **D**, desipramine. The sensorgrams were obtained from the ligand channels of POPC and DSPC/CHOL (NH₄)₂SO₄. The two liposomes were captured to the level of 7,800 RU and 8,900 RU, respectively. The small molecule drugs were injected in a twofold dilution series ranging from 500 μM to 31 μM. The maximum responses in the sensorgrams are plotted against the analyte concentrations for each liposome-drug interaction. DSPC/CHOL (NH₄)₂SO₄ (—); POPC (—). RU, response units.

In order to further characterize the liposome–small molecule interactions in this drug delivery model, the correlation between maximum responses in analyte injections and liposome surface densities was investigated. Surfaces with two types of liposomes, POPC and DSPC/CHOL (NH₄)₂SO₄, were employed. Multiple small molecule drugs were used as analytes. In addition, the two surface chemistries for capturing liposomes — the conventional lipophilic surface chemistry (by ProteOn GLC lipid kit) and the novel hydrophilic surface chemistry (by ProteOn liposome capturing kit) — were compared. The results

are shown in Figure 7. When the lipophilic surface chemistry was applied, a GLC sensor chip was used and the variation of liposome surface densities was realized by changing the surface lipophilicity. When the hydrophilic surface chemistry was applied, an LCP sensor chip was used and the variation of liposome surface densities was realized by using one, two, or three layers of liposomes. The linearity between maximum responses in analyte injections and liposome surface densities is observed in all cases.

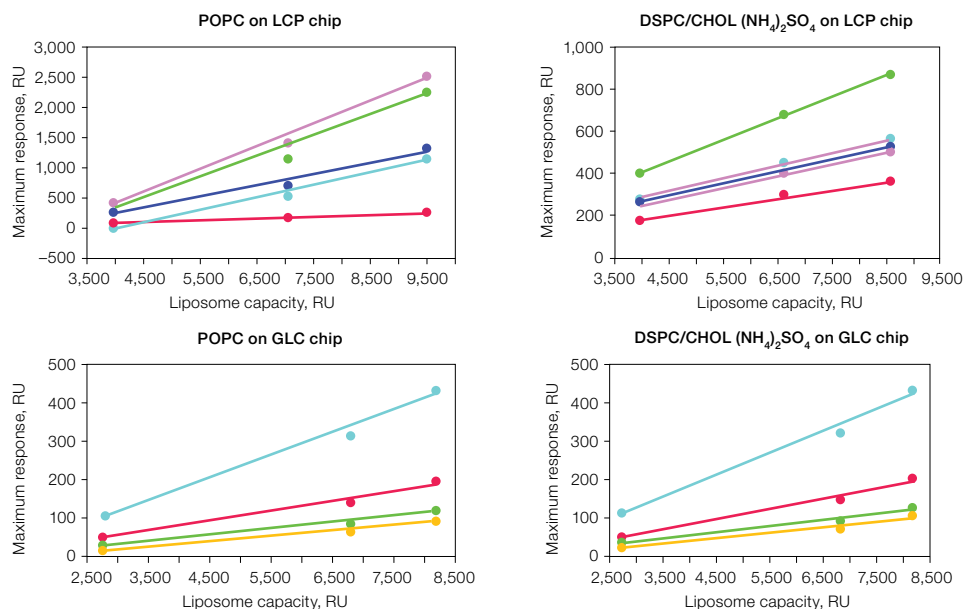


Fig. 7. Maximum responses in analyte injections in correlation with the surface density of liposomes.

Different liposome surface densities were prepared on the two surface chemistries, using the ProteOn liposome capturing kit and the ProteOn GLC lipid kit. Two liposomes, POPC and DSPC/CHOL (NH₄)₂SO₄, were captured on chip surfaces and multiple small molecule drugs were injected at the concentration of 0.5 mM. The injection time was set at 180 sec, and the flow rate for liposome capture was 25 µl/min. The linearity between maximum responses and liposome surface densities is shown. alprenolol 0.5 mM (●); propranolol 0.5 mM (●); dibucaine 0.5 mM (●); imipramine 0.5 mM (●); despiramine 0.5 mM (●); verapamil 0.5 mM (●). RU, response units.

While both the lipophilic and hydrophilic surface chemistries showed very good performance in the liposome–small molecule interaction analysis, the absolute values of responses in analyte injections were significantly different between the GLC and LCP sensor chips. At similar liposome surface densities, most absolute values of responses are several-fold higher on the LCP sensor chip using the ProteOn liposome capturing kit. An explanation is that the DNA linker between liposomes and the chip surface reduces the steric hindrance to access the entire surface of a liposome particle. Also, the hydrophilic surface chemistry is beneficial for maintaining intact liposomes, which further guarantees the data quality in applying this drug delivery model. This advantage results in higher performance of the novel hydrophilic surface chemistry compared with the conventional liposome capture method.

Conclusion

The application results demonstrate excellent performance of the ProteOn liposome capturing kit in the label-free analysis of liposome–small molecule interactions. The novel hydrophilic surface chemistry for liposome capture shows excellent performance in controlling liposome surface densities and maintaining accurate interaction analysis. Utilizing the One-shot Kinetics™ approach, dose-response sensorgrams were successfully and efficiently obtained for further characterization.

The comparison with the conventional liposome capture method positions this novel method as an advanced solution for liposome applications in SPR biosensors. Thus, the combination of the novel surface chemistry and the ProteOn XPR36 system is able to extend SPR technology to the liposome-based small molecule drug delivery analysis.

Reference

- Baird CL et al. (2002). Surface plasmon resonance characterization of drug/liposome interactions, *Anal Biochem* 310, 93–99.
- Balon K et al. (1999). Drug liposome partitioning as a tool for the prediction of human passive intestinal absorption, *Pharm Res* 16, 882–888.
- Barenholz Y (2006). Amphipathic weak base loading into preformed liposomes having a transmembrane ammonium ion gradient: from the bench to approved Doxil. *Liposome Technology, Vol II (3rd Edition) 2*, 1–25.
- Buchwald P and Bodor N (1998). Octanol-water partition: searching for predictive models, *Curr Med Chem* 5, 353–380.
- Danelian E et al. (2000). SPR biosensor studies of the interaction between 27 drugs and a liposome surface: correlations with fraction absorbed in humans, *J Med Chem* 43, 2083–2086.

Biacore is a trademark of GE Healthcare.

The ProteOn XPR36 protein interaction array system is covered by Bio-Rad patents, including United States patent numbers 8,111,400, 8,105,845, 7,999,942, and 7,443,507.

This product or portions thereof is manufactured and sold under license from GE Healthcare under United States patent numbers 5,492,840, 5,554,541, 5,965,456, 7,736,587, and 8,021,626, and any international patents and patent applications claiming priority.



BIO-RAD

**Bio-Rad
Laboratories, Inc.**

Life Science
Group

Web site www.bio-rad.com **USA** 800 424 6723 **Australia** 61 2 9914 2800 **Austria** 01 877 89 01 **Belgium** 09 385 55 11 **Brazil** 55 11 5044 5699
Canada 905 364 3435 **China** 86 21 6169 8500 **Czech Republic** 420 241 430 532 **Denmark** 44 52 10 00 **Finland** 09 804 22 00
France 01 47 95 69 65 **Germany** 089 31 884 0 **Greece** 30 210 9532 220 **Hong Kong** 852 2789 3300 **Hungary** 36 1 459 6100 **India** 91 124 4029300
Israel 03 963 6050 **Italy** 39 02 216091 **Japan** 03 6361 7000 **Korea** 82 2 3473 4460 **Mexico** 52 555 488 7670 **The Netherlands** 0318 540666
New Zealand 64 9 415 2280 **Norway** 23 38 41 30 **Poland** 48 22 331 99 99 **Portugal** 351 21 472 7700 **Russia** 7 495 721 14 04
Singapore 65 6415 3188 **South Africa** 27 861 246 723 **Spain** 34 91 590 5200 **Sweden** 08 555 12700 **Switzerland** 026 674 55 05
Taiwan 886 2 2578 7189 **Thailand** 800 88 22 88 **United Kingdom** 020 8328 2000